

# Development and Preliminary Results of a Large-Pixel Two-Layer LaBr<sub>3</sub> Compton Camera Prototype

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**Abstract:** *Objective.* Lanthanum bromide (LaBr<sub>3</sub>) crystal has a high energy resolution and time resolution and has been used in Compton cameras (CCs) over the past few decades. However, LaBr<sub>3</sub> crystal arrays are difficult to process because LaBr<sub>3</sub> is easy to crack and break; thus, few LaBr<sub>3</sub>-based CC prototypes have been built. In this study, we designed and fabricated a large-pixel LaBr<sub>3</sub> CC prototype and evaluated its performance with regard to position, energy, and angular resolution. *Approach.* We used two 10 × 10 LaBr<sub>3</sub> crystal arrays with a pixel size of 5 mm × 5 mm, silicon photomultipliers (SiPMs), and corresponding decoding circuits to construct our prototype. Additionally, a framework based on a Voronoi diagram and a lookup table was developed for list-mode projection data acquisition. Monte Carlo (MC) simulations based on Geant4 and experiments were conducted to evaluate the performance of our CC prototype. *Main results.* The lateral position resolution was 5 mm, and the maximum deviation in the depth direction was 2.5 and 5 mm for the scatterer and absorber, respectively. The corresponding measured energy resolutions were 7.65% and 8.44%, respectively, at 511 keV. The experimental results of <sup>137</sup>Cs point-like sources were consistent with the MC simulation results with regard to the spatial positions and full widths at half maximum (FWHMs). The angular resolution of the fabricated prototype was approximately 6° when a point-like <sup>137</sup>Cs source was centrally placed at a distance of 5 cm from the scatterer. *Signification.* We proposed and investigated a large-pixel LaBr<sub>3</sub> CC for the first time and verified its feasibility for use in accurate spatial positioning of radiative sources with a high angular resolution. The proposed CC can satisfy the requirements of radiative source imaging and positioning in the nuclear industry and medical applications.

**Keywords:** Compton camera, large pixel, gamma camera, LaBr<sub>3</sub> detector, prototype evaluation.

## 1. Introduction

To overcome the low detection efficiency of traditional image-forming systems for high-energy gamma rays, the Compton camera (CC) was proposed in 1974 [1]. The CC uses electronic collimation rather than mechanical collimation; therefore, it has a wider field of view (FOV) and higher detection efficiency. It can be used for detecting gamma rays over a wide energy range of 100 keV–10 MeV, which covers natural radioactivity of nuclear materials and waste [2–4] and the typical gamma-ray energy used in medical applications such as

radiopharmaceutical imaging [5–8] and prompt gamma imaging [9–11]. The earliest prototype of a CC was a single-layer system that could distinguish the photon scattering position and the photon absorbed position with a single layer of scintillator detector. However, owing to the limitations of the detector material and data-acquisition technology, the CC was not applied in practice.

To improve the performance of the CC, several CC prototypes have been proposed and built over the past few decades. CC prototypes can be divided into two main categories: single-layer and multilayer. The single-layer CCs are similar to the earliest CCs prototypes but are based on the latest developments of detector materials and circuit readout technology. Among them, the three-dimensional (3D) cadmium zinc telluride (CZT) CC is the representative single-layer CC. Considerable research on the 3D CZT CC has been performed, and prototypes have been developed [12]. Single-layer CCs have the advantages of a large FOV of  $4\pi$ , high spatial resolution, and high energy resolution; however, the detector material is expensive. Additionally, the distance between the scattering position and the absorbed position is far shorter than that in multilayer CC, resulting in a larger deviation of the spatial orientation of Compton cones. Multilayer CCs determine the scattering position and the absorbed position in separated detectors; thus, only photons incident in a specific direction are received. Multilayer CCs have been developed and used in the detection of radioactive materials [13] and prompt gamma imaging during hadron therapy [14]. Among the multilayer CCs, three or more-layer CCs have a high detection efficiency, but they are more expensive than two-layer CCs while having comparable performance, and the probability of three-point interaction events is far lower than that of two-point interaction events [15]. Thus, two-layer CCs are the mainstream prototypes for multilayer CCs.

The scintillator materials used in CCs have been researched in the past few years [16–19]. The scintillator material has relatively high detection efficiency and time resolution. There are many types of scintillators, such as LYSO, GAGG, and lanthanum bromide ( $\text{LaBr}_3$ ). Each has advantages and disadvantages. Thus, different scintillators have been used in CCs for different purposes. LYSO and GAGG crystals have higher densities (7.2 and 6.6 g/cm<sup>3</sup>, respectively) than  $\text{LaBr}_3$ . However, LYSO has background radiation ranging from 88 to 597 keV, which reduces the energy resolution—particularly for detecting natural radioactivity [20]. Additionally, GAGG has a long light decay time of approximately 90 ns, making it easier to obtain an error coincidence energy signal compared with the 20-ns coincidence time window used in this study. The  $\text{LaBr}_3$  scintillator has a light decay time of 20 ns and relatively low intrinsic background radiation. Moreover, it has the highest energy resolution among the three outstanding and cost-effective scintillators. Extensive research has been conducted on the  $\text{LaBr}_3$  scintillator owing to its excellent performance [21–24]. Therefore, it was used in our CC prototype in this study.

The existing CC prototypes usually have a small pixel size (e.g., 1 mm × 1 mm) and a large number of pixels in every layer (e.g., several hundreds of pixels per layer) for obtaining accurate

reconstruction results. There has been little research on the influence of the large pixel size of the CC on the reconstruction accuracy. Additionally, the LaBr<sub>3</sub> crystal is easy to crack and break during processing, making it difficult to obtain small-pixel size LaBr<sub>3</sub> crystal arrays. Among the research on LaBr<sub>3</sub>-based CCs, only MACACO had a small pixel size (3 mm × 3 mm) [15]. Although a large pixel size leads to a low position resolution, one promising solution is using the reconstruction algorithm with resolution recovery (RR). Recently, RR-based reconstruction algorithms have proven to be useful in correcting the error caused by the limited resolutions of actual CCs [25, 26]. Among them, RR-based maximum likelihood expectation-maximization (MLEM) [6] and origin ensemble (OE) [7] algorithms have attracted considerable attention, and optimization methods such as graphics processing unit (GPU) acceleration [6] and deep learning [8] have been applied. Additionally, radioactive source imaging with a CC prototype during nuclear decommissioning based on the subset-driven origin ensemble with resolution recovery (SD-OE-RR) algorithm was demonstrated [3]. Thus, CC systems with large pixel sizes are expected to reconstruct images with a high spatial resolution with the help of RR-based reconstruction algorithms, making them promising for practical applications.

In this study, we developed and evaluated a two-layer LaBr<sub>3</sub> CC prototype with a large pixel size for nuclear material and waste detection. Two LaBr<sub>3</sub> crystal arrays with a relatively large pixel size of 5 mm × 5 mm × 5 (10) mm, silicon photomultipliers (SiPMs), and coding circuits were used to construct our prototype. We used a data-acquisition card (DAQ) to select and decode the coincidence events and developed a framework to obtain the list-mode data from time-series projection data including the interaction positions and energies deposited in the scatterer and absorber. Finally, we evaluated the performance of our prototype via simulations and preliminary experiments.

## 2. Materials and Methods

### 2.1 Structure of two-layer LaBr<sub>3</sub> Compton camera prototype

The LaBr<sub>3</sub> CC prototype consisted of a scatterer and an absorber, both of which had the same cross-sectional area. As shown in Figure 1, the LaBr<sub>3</sub> detectors consisted of a 10 × 10 LaBr<sub>3</sub> array with a thickness of 5 mm for the scatterer and 10 mm for the absorber (Kinheng Crystal, Shanghai, China) and a coding circuit module that contained the SiPM (TOFTEK, Wuxi, China). The pixel size of the LaBr<sub>3</sub> array was 5 mm × 5 mm × 5 (10) mm, and the pixels were separated by a 0.1-mm BaSO<sub>4</sub> spacer. A 1-mm-thick glass plate and a 1.2-mm-thick Al shell were used for vacuum packing. The volume of the LaBr<sub>3</sub> array was 56.4 mm × 56.4 mm × 9.3 (14.3) mm. Both layers had a coding circuit module behind the scintillator arrays, which included an 8 × 8 array of SiPMs and a 4-channel output encoding circuit. The voltage values of the 64-channel signals output from the SiPMs were proportional to the number of scintillating photons distributed in the corresponding area of 64 SiPM pixels. The 4-channel output encoding circuit transferred the 64-channel signals of the SiPMs to the 4-channel output through a resistance weight network.

Finally, the output signals were input into the DAQ (TOFTEK, Wuxi, China). The eight signals (four channels from the scatterer and four channels from the absorber) were input into the same DAQ simultaneously, and the DAQ output the total voltage values of the eight signals in every time window. The two layers were fixed by a 3D-printed resin bracket. The distance between the center of the two  $\text{LaBr}_3$  arrays was adjustable, and the default value was 50 mm.

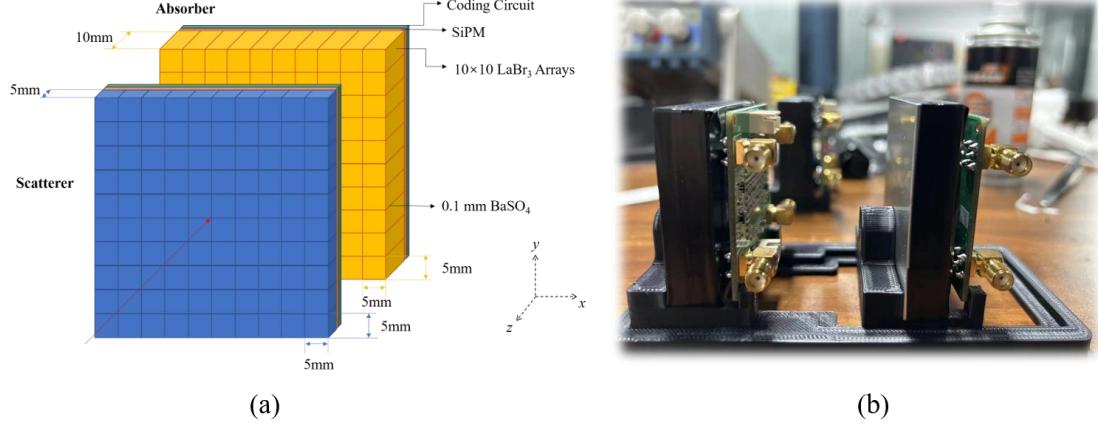


Figure 1. Fabricated two-layer  $\text{LaBr}_3$  CC prototype: (a) structure diagram; (b) photograph.

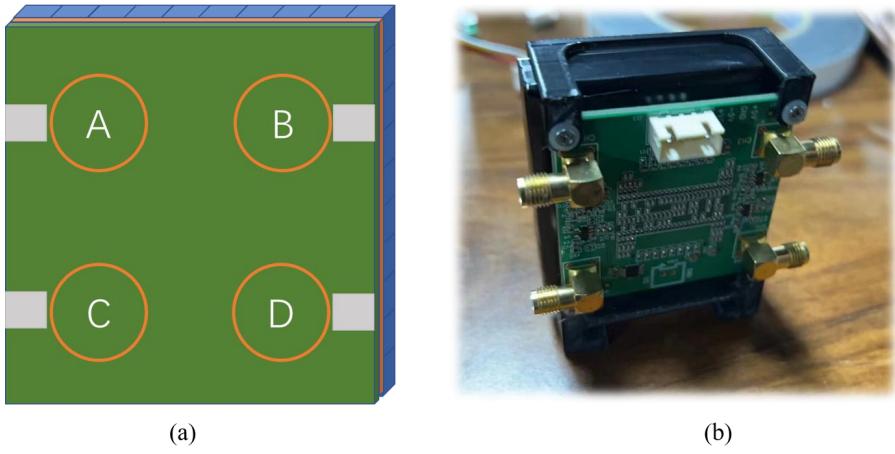


Figure 2. Encoding circuit and position decoding diagram: (a) structure diagram of the  $\text{LaBr}_3$  CC detector; (b) photograph of the  $\text{LaBr}_3$  detector.

## 2.2 List-mode data acquisition through lookup table

The DAQ output a row of data including nine integers: a timestamp and  $V_1$ – $V_8$ .  $V_1$ – $V_8$  were the eight voltage signals;  $V_1$ – $V_4$  were the scatterer voltage signals, and  $V_5$ – $V_8$  were the absorber voltage signals. The subscripts from smallest to largest corresponded to A, B, C, and D in Figure 2.

The positions in scatterplots ( $x_{V_1}, y_{V_1}, x_{V_2}, y_{V_2}$ ) where the scintillating photons were generated and received were calculated via the method used in the Anger camera [27].

$$x_{V_1} = \frac{V_1 - V_3 + V_2 - V_4}{V_1 + V_2 + V_3 + V_4} \cdot \rho$$

(1)

$$y_{V-1} = \frac{V-1-V}{V-1+V} \frac{2+V}{2+V} \frac{3-V}{3+V} \frac{4}{4} \cdot \rho$$

(2)

$$x_{V-2} = \frac{V-5-V}{V-5+V} \frac{7+V}{6+V} \frac{6-V}{7+V} \frac{8}{8} \cdot \rho$$

(3)

$$y_{V-2} = \frac{V-5-V}{V-5+V} \frac{6+V}{6+V} \frac{7-V}{7+V} \frac{8}{8} \cdot \rho$$

(4)

Here,  $\rho$  is the gain factor used to discretize the interaction positions. By default, we set  $\rho = 0.78125$ , and the corresponding  $512 \times 512$  pixelated space was used to store and display the original scatterplot.

Because the responses to the scintillating photons varied among different crystals and positions, the original scatterplot did not exhibit a standard scattered point array. A connection between the initial scatterplots and the pixel coordinates of the crystal arrays was established via the following steps. The original scatterplot was subjected to image processing, e.g., enhancement, denoising, and smoothing, whereby the most representative positions of different scatters were found and marked with a crystal index. Then, a Voronoi diagram whose seed points were the selected positions was created according to the principle of the minimum distance between position seeds and every point in the scatterplot [28]. Using the diagram, a lookup table (LUT) of photon events' decoded positions and corresponding crystal indices was constructed. Through the LUT, the acting positions of gamma photons were efficiently determined. In the study, we used the center coordinates of the crystal pixel to represent the spatial position where the gamma photon interacted with the detectors to achieve the optimal estimation. Thus, the lateral position resolution was 5 mm, and the maximum deviation in the depth direction was 2.5 and 5 mm for the scatterer and absorber, respectively.

The next step was to obtain the energy responses of different crystals. The sum of the voltage signals of all the layers is the address of the channel in the energy spectrum. Every crystal unit must be calibrated using the following formula:

$$e_{i,j} = a_{i,j} + b_{i,j} \cdot \sum_{c=4(j-1)+1}^{c=4j+1} V_c, \quad j = 1 \text{ or } 2, \quad (5)$$

where  $e_{i,j}$  represents the deposited energy in the  $i^{\text{th}}$  pixels of the  $j^{\text{th}}$  layer, and

$a_{i,j}$  and  $b_{i,j}$  are the parameters. Three types of natural radioactive sources ( $^{22}\text{Na}$ ,  $^{57}\text{Co}$ , and  $^{137}\text{Cs}$ ) and their four characteristic energies were used for energy calibration.

For every two-point event, the output list-mode data were in the format of  $(x_1, y_1, z_1, e_1, x_2, y_2, z_2, e_2)$ . Here,  $x_1, y_1, z_1$

represented the interaction position in the scatter.  $x_1$  and  $y_1$  represented the lateral position depending on the crystal pixel the event clustered to.  $z_1$  represented the position in the depth direction and was set as a constant (0 mm).  $x_2, y_2, z_2$  represented the interaction position in the absorber, and  $z_2$  was set to -50 mm. In some cases,  $L_1$  and  $L_2$  were used to replace  $x_1, y_1, z_1$  and  $x_2, y_2, z_2$ , respectively.  $e_1$  and  $e_2$  represented the deposited energy in the scatterer and absorber, respectively, calculated via Equation (5).

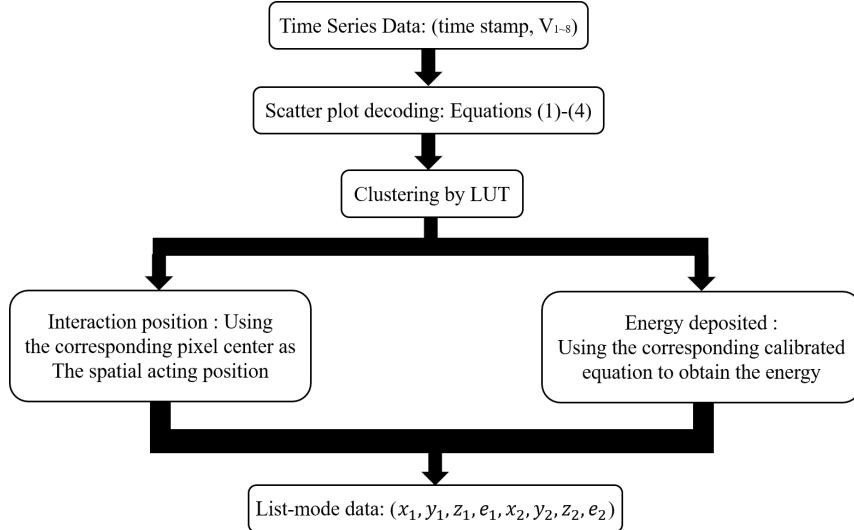


Figure 3. Framework of the list-mode projection data acquisition for the prototype.

As the developed prototype is expected to be used in detecting sources that may emit photons of different energies, event selection methods are used in projection data acquisition to obtain the valid events used for reconstruction. In our study, the characteristic energy window depended on prior knowledge, or the measured energy spectrum was used to select events with certain total deposited energies for corresponding radioactive sources. In addition, if only locating the radioactive sources and reconstructing the relative activity were needed, a large energy window that covered all the characteristic energies but eliminated noise was allowed, because the CC could reconstruct the locations and activities of sources where photons with different energies would make equal contributions in the formula of back projected Compton cones.

### 2.3 Reconstruction algorithm

In this study, the previously proposed SD-OE-RR algorithm was used for reconstruction [3]. It is an optimized origin ensemble (OE) algorithm that was developed for CC reconstruction in a large FOV with a projected coordinate system ( $\theta_x, \theta_y, z$ ) during nuclear decommissioning source term investigation, and it can also be used to evaluate the angular resolution of the proposed LaBr<sub>3</sub> CC prototype. The OE algorithm has been proven to have the same estimate as the MLEM algorithm under some approximation [29]. However, OE algorithms

have reconstruction speeds several orders of magnitude higher than that of the MLEM algorithm [26].

OE algorithms use transitions of different states as the iterative process. In a typical case of locating gamma rays, the detector with  $K$  bins receives  $I$  events from the image volume divided into  $J$  voxels. States can be defined as the locations of  $I$  events assigned to  $J$  voxels individually; in this case, there are  $J^I$  states. The reconstruction process finds the most probable state. The probability of a certain state  $s$  was defined as the product of the probability that events emitting in the certain voxel, as follows:

$$P(s) = \prod_{i=1}^I p_{s_i j}, \quad (6)$$

where  $P(s)$  represents the probability of state  $s$ , and  $p_{s_i j}$  represents the probability that the origin of event  $i$  is located in voxel  $j$  (while event  $i$  was thought to be located in voxel  $j$  in state  $s$ ).  $p_{s_i j}$  can be defined as follows:

$$p_{s_i j} = \alpha_{k_i j} n_{s_j} / \varepsilon_j, \quad (7)$$

where  $\alpha_{k_i j}$  represents the probability that event  $i$  detected in bin  $k$  emits in voxel  $j$ , which is the differential cross section of the current scattering angle and is calculated via the Klein–Nishina formula in the CC system.  $n_{s_j}$  represents the number of events whose origin is in voxel  $j$  in state  $s$ , and  $\varepsilon_j$  represents the sensitivity of voxel  $j$  to the detector. Thus,  $n_{s_j} / \varepsilon_j$  is the estimate of the activity of voxel  $j$  in state  $s$ . In this case, Equation (6) can be rewritten as

$$P(s) = \prod_{i=1}^I \alpha_{k_i j} n_{s_j} / \varepsilon_j. \quad (8)$$

Because  $n_{s_j}$  is the sum of events that are thought to emit in voxel  $j$ , for calculating  $P(s)$ , the activity of voxel  $j$  is multiplied for  $n_{s_j}$  times. Equation (8) can thus be rewritten as

$$P(s) = \prod_{i=1}^I \alpha_{k_i j} \prod_{j=1}^J (n_{s_j} / \varepsilon_j)^{n_{s_j}}. \quad (9)$$

A higher  $P(s)$  indicates that the state is closer to the optimal estimation; thus, the OE algorithm iterates by comparing the probabilities of two adjacent states and transforming the current state. Here, “adjacent states” refers to two states that differ in the location of only one event. The probability ratio can be simplified as follows:

$$\frac{P(s')}{P(s)} = \frac{\alpha_{k_i j} \cdot (n_{s_j} - 1)^c \cdot s_j^{-1} \cdot (n_{s_{j'}} + 1)^n \cdot s_{j'}^{+1} / \varepsilon_{j'}}{\alpha_{k_i j} \cdot (n_{s_j})^n \cdot s_j \cdot (n_{s_{j'}})^n \cdot s_{j'} / \varepsilon_{j'}}. \quad (10)$$

For the CC system, an event only emits on the Compton cone; thus,  $\alpha_{k_i j}$  is equal to either  $\alpha_{k_i j}$  or 0. In the latter case, voxel  $j'$  is not on the Compton cone, and  $\frac{P(s')}{P(s)} = 0$ . In the former case,  $j$  and  $j'$  are on the same Compton cone, and the sensitivities of all the voxels are approximately equal for the far-field reconstruction. Thus, these parts can be canceled. Additionally, the following approximation can be made:  $(1 \pm \frac{1}{c})^c \approx e^{\pm 1}$ . When  $c \gg 1$ , the probability ratio can be simplified as follows:

$$\frac{P(s')}{P(s)} = \frac{n_{s_{j'}}}{n_{s_j}} \text{ or } \frac{P(s')}{P(s)} = \frac{n_{s_{j'}} + 1}{n_{s_j}}. \quad (11)$$

Usually, the initial estimate of activity has no restrictions, but a more accurate initial state will lead to a higher convergence rate and a better reconstruction result. In the OE algorithm, events are stochastically assigned to the voxel that is on the corresponding Compton cone as an initial state. However, owing to the finite energy resolution and position resolution of the detector and the Doppler broadening effect, the Compton cone calculated using the list-mode data cannot cover all the possible voxels where the event really emitted. In the SD-OE-RR algorithm, these effects on the angular resolution are considered. The influence of the energy resolution and the Doppler effect on the deviation of the calculated scattering angle can be expressed as follows [3]:

$$\Delta(\cos \theta_i)_r \approx \frac{m_0 c^2}{E^2} \cdot \delta \cdot \left(1 + \frac{\Delta E_{doppler}^2}{2\Delta E_{2s}^2}\right), \quad (12)$$

where  $\delta$  represents the energy resolution of the detectors, and  $E_{2s}$ ,  $\Delta E_{2s}$ , and  $\Delta E_{doppler}$  represent the deposited energy in the absorber, the energy deviation of the deposited energy in the absorber in terms of statistical fluctuations, and the energy deviation caused by the Doppler broadening effect, respectively.  $m_0 c^2$  represents the static energy of the electron. For the position resolution, the effects of the interaction position deviation on the deviation of the scatter angle can be expressed as follows [30]:

$$\Delta \theta_{i_g} = \sqrt{\frac{\Delta l^2 (1 + k \cos \theta_i)^2 + (\Delta z_s \cdot k \sin \theta_i)^2}{|\mathbf{v}_{j'} \cdot \mathbf{L}_{i-1}|^2} + \frac{c \cos \theta_i^2 \theta_{i-1}^2 ((\Delta l \cos \theta_i)^2 + (\Delta z_s \sin \theta_i)^2)}{|\mathbf{L}_{i-1} \cdot \mathbf{L}_{i-2}|^2}}, \quad (13)$$

where  $\overrightarrow{v_j L_{i-1}}$  is a vector consisting of voxel  $v_j$  in the FOV and interaction position  $L_{i-1}$  in the scatterer, and  $\overrightarrow{L_{i-1} L_{i-2}}$  is a vector consisting of the interaction position  $L_{i-1}$  in the scatterer and the interaction position  $L_{i-2}$  in the absorber of the  $i^{\text{th}}$  event.  $\theta_i$  represents the scattering angle determined by the deposited energies in the scatterer and absorber.  $\Delta l$  represents the lateral position resolution.  $\Delta z_s$  and  $\Delta z_a$  represent the position resolutions along the depth directions of the scatterer and absorber, respectively.  $k$  represents the ratio of the distance between the source and the interaction position in the scatterer to the distance between the interaction positions in the scatterer and the absorber, that is,  $\frac{\overrightarrow{v_j L_{i-1}}}{\overrightarrow{L_{i-1} L_{i-2}}}$ . The total deviation of the scattering angle is the geometric mean of the aforementioned effects.

$$\Delta \cos \theta_i = \sqrt{\Delta(c \cos \theta_i)_r^2 + \Delta(c \cos \theta_i)_g^2} \quad (14)$$

In contrast to the OE algorithm, the SD-OE-RR algorithm stores all the voxels' indices (subsets of the OEs) by traversing all possible voxels of photon events with the cones and deviations via Equation (15).  $\Delta(\cos \theta_i)$  was 0.06 for the fabricated LaBr<sub>3</sub> CC prototype, as given by Equations (12)–(14).

$$S_{O_{i,j}} = \left\{ (v_j) \mid \left| \frac{\overrightarrow{v_j L_{i-1}} \cdot \overrightarrow{L_{i-1} L_{i-2}}}{\| \overrightarrow{v_j L_{i-1}} \| \| \overrightarrow{L_{i-1} L_{i-2}} \|} - c \cos \theta_i \right| \leq \frac{\Delta(c \cos \theta_i)}{2.355} \right\} \quad (15)$$

After a back projection process of  $S_{O_{i,j}}$  with an equal weight of 1, the initial estimate of the activity distribution considering the resolution effects can be obtained as follows:

$$f_{0j} = \sum_i S_{O_{i,j}}. \quad (16)$$

The iterative process of the SD-OE-RR algorithm is given by Equations (17) and (18).

$$f_{n+1,j-i} = \max\{\text{sgn}(f_{n,j-i} - f_{n,j-i}) \cdot \text{sgn}(\frac{f_{n,j-i+1}}{f_{n,j-i}} - r_{n+1}) \cdot (f_{n,j-i} + 1),$$

$$\text{sgn}(f_{n-j-i} - f_{n-j-i'}) \cdot \text{sgn}(r_{n+1} - \frac{f_{n-j-i'}+1}{f_{n-j-i}}) \cdot (f_{n-j-i'} - 1) \} \quad (17)$$

$$f_{n+1-j-i} = \max\{\text{sgn}(f_{n-j-i} - f_{n-j-i'}) \cdot \text{sgn}(\frac{f_{n-j-i'}+1}{f_{n-j-i}} - r_{n+1}) \cdot (f_{n-j-i'} - 1), \\ \text{sgn}(f_{n-j-i} - f_{n-j-i'}) \cdot \text{sgn}(r_{n+1} - \frac{f_{n-j-i'}+1}{f_{n-j-i}}) \cdot (f_{n-j-i'} + 1) \} \quad (18)$$

Here,  $f_{n-i}$  represents the count in voxel  $i$  in the  $n^{\text{th}}$  iteration, and  $j_{-i}$  and  $j_{-i'}$  represent the positions of event  $i$  in the current state and the proposed new state, respectively.  $r_{n+1}$  is a random number in the range of 0–1 used in the  $(n+1)^{\text{th}}$  iteration.  $\text{sgn}(x)$  denotes the signum function, which equals  $-1$  when  $x < 0$  and  $1$  when  $x > 0$ . The implementation steps are presented below [31].

Step 1: Calculate the deviations  $\Delta(c \circ s \theta)$  of all photon event cones by using Equation (14) with the position and energy uncertainties and the Doppler broadening effect. Use Equation (15) to obtain the subsets of the OEs of event  $i$ .

Step 2: Use the sum of all the initial event counts of the voxels in  $S O_{-i-j}$  as an initial estimate of the source distribution.

Step 3: Randomly select one event  $i$ . Randomly select a new location (i.e., voxel  $j'$ ) of this event in the  $i^{\text{th}}$  row vector of  $S O_{-i-j}$  for state  $s'$ . Obtain the corresponding event counts  $n_{-j'}$  and  $n_{-j}$  of the voxel where event  $i$  is located for states  $s$  and  $s'$ , respectively.

Step 4: Determine the acceptance probability  $A$  for the new location of event  $i$  by using Equation (16) and generate a random number  $\alpha$  uniformly distributed between 0 and 1.

$$A = \min [1, \frac{(n_{-j'}+1)}{n_{-j}}] \quad (16)$$

Step 5: Event  $i$  moves to the new location if  $A > \alpha$  and remains at the current location if  $A \leq \alpha$ . The voxel where event  $i$  is located after the above operation becomes the old location of the next iteration, and the corresponding event counts of the voxels in  $S O_{-i-j}$

are updated.

Step 6: Repeating Steps 2–4  $N$  times corresponds to one full iteration of the algorithm. After a sufficient number of iterations ( $3 \times 10^6$ ), the event counts in the voxels are approximately invariant, and the reconstructed image is obtained by summing all the weights of the same voxel in the sparse matrix  $S O_{i, j}$ .

## 2.4 Monte Carlo simulation

Geant4 p10.03 was used to model the CC with the same structure and position and energy resolutions as the fabricated CC prototype. The Doppler broadening effect was included in the simulations. Four simulations were conducted to evaluate the angular resolutions of the CC with different angles, distances, source areas, and source energies.

- i) Angular resolutions with different angles: An ideal point-like source was placed at 25 positions along the lateral and diagonal directions in the FOV. The distance between the source and the scatterer of the CC was 10 cm.
- ii) Angular resolutions with different distances: An ideal point-like source was placed at the center of the FOV, and the distance between the source and the scatterer of the CC was varied from 5 cm to 1 m.
- iii) Angular resolutions of sources with different areas: Circular plane sources with radii varying from 0.5 to 5 cm were placed at the center of the FOV, and the distance between the source and the scatterer of the CC was 10 cm.
- iv) Angular resolutions of sources with different energies: An ideal point-like source was placed at the center of the FOV. The energy of the source was set as 511, 662, and 1275 keV for single-energy source simulation. For multiple-energy sources, the energy of the source was set as a combination of two of the aforementioned three energies, with each energy accounting for 50%. Another combination of 64.3% 511 keV and 35.7% 1275 keV was used as an imitation of a real  $^{22}\text{Na}$  source. The distance between the source and the scatterer of the CC was 5 cm. Because the variation caused by the deviation of the energy was relatively small, a short distance would amplify the variation and make it more perceptible.

Approximately 10000 events were used for reconstruction in each simulation. The projection data obtained in the simulations considered the position resolution and energy resolution of the CC, which were consistent with the fabricated prototype, as well as the Doppler broadening effect. The lateral positions of the events were moved to the center coordinates of the nearest pixels. The positions in the depth direction were set as 0 or -50 mm for the scatterer and absorber. The deposition energy was degraded by Gaussian noise representing the uncertainty caused by the Doppler broadening effect and energy resolution. As the noise and the simulation data were stochastic, the results were the averages of five reconstructions under the same condition.

The aforementioned angular resolution was defined as follows in a plane coordinate system [32]:

$$\sigma_{\theta} = a \cdot r \cdot c \cdot t \cdot a \cdot n \quad \left( \frac{\text{FWHM}_0}{d} \right) \quad (17)$$

where  $\text{FWHM}_0$  represents the mean value of the full widths at half maximum (FWHMs) in the profiles taken from different angles through the source, and  $d$  represents the distance between the source and the scatterer. For the projected coordinate system used in this study, Equation (17) was transformed into

$$\sigma_{\theta} = \text{FWHM}_a \cdot c \cdot o \cdot s \cdot \varphi \quad (18)$$

where  $\text{FWHM}_a$  has a similar definition to  $\text{FWHM}_0$  except that  $\text{FWHM}_a$  was measured in projected coordinates with the unit of degrees,  $\varphi$  represents the angle between the Z-axis and the line passing through the source and the center of the scatterer. For convenience, the FWHM is used to represent  $\sigma_{\theta}$  hereinafter, and it has units of degrees.

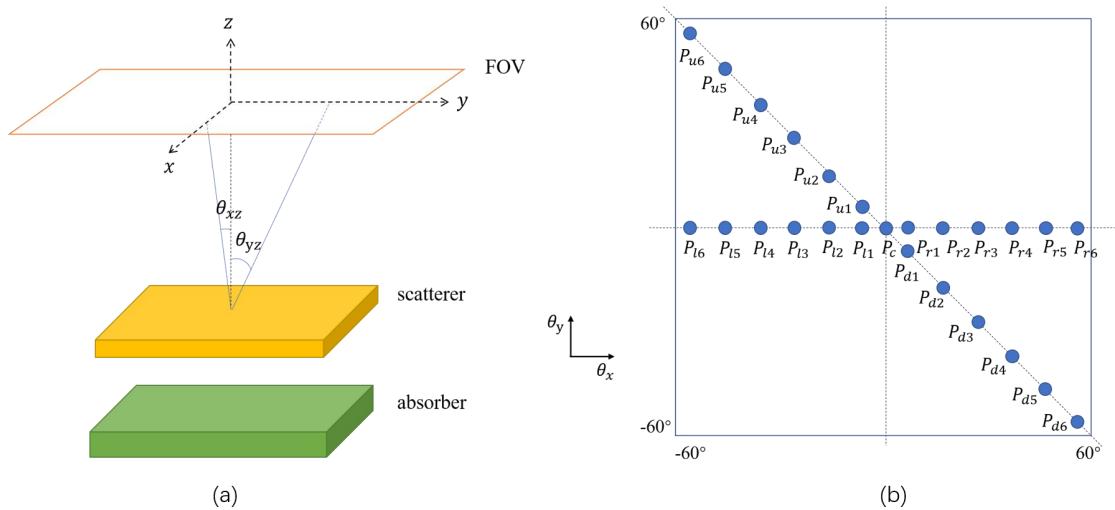


Figure 4. (a) Setup of the LaBr<sub>3</sub> CC in the simulation. (b) Schematic of simulated ideal point-like sources in the FOV.

## 2.5 Experiments

In the experiments, a point-like <sup>137</sup>Cs source with activity of approximately 9000 Bq was placed at three positions matching those used in the simulations labeled  $P_{l1}$ ,  $P_{l2}$ ,  $P_{c1}$ , and  $P_{d1}$ . The distance between the source and the scatterer of the prototype was 5 cm. Each measurement took 5 min. The numbers of obtained coincident events with a total energy of 600–700 keV were 315, 360, and 205, respectively.

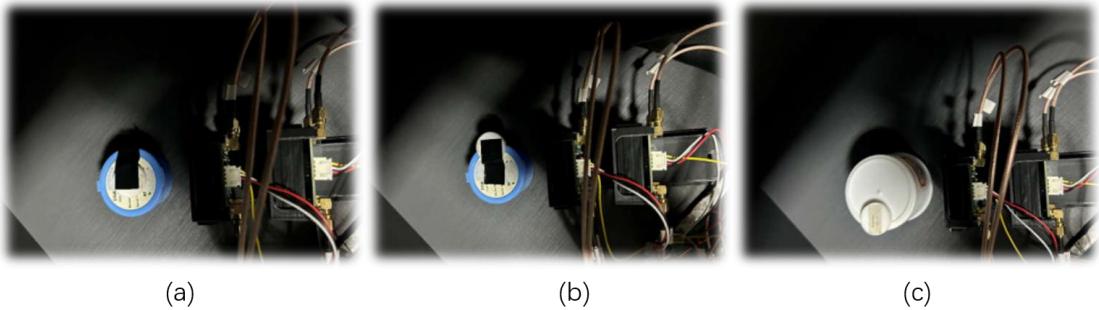


Figure 5.  $^{137}\text{Cs}$  point-like source imaging experiments involving the  $\text{LaBr}_3$  CC prototype at three positions.

### 3. Results

#### 3.1 Position decoding and energy spectrum calibration

The scatterplots of the scatterer and absorber constructed using the detection results of the  $^{22}\text{Na}$  source are shown in Figure 6. An LUT was created after numbering all the centroids, providing a fast-clustering method. The distances between all the pixel points in the scatterplots and every centroid of the point group were compared, each pixel was labeled with the number of the nearest centroid. Two Voronoi diagrams of each layer are shown in Figures 6(c) and (d). In the diagrams, the scatterplots are segmented by the white line, indicating that any event decoded in a single area would be clustered to the corresponding scatter and pixel. The final decoding interaction positions of all the events are also shown in Figure 6.

To obtain the total energy response of the scatterer and absorber, the energy responses of every crystal were measured and calibrated.  $^{22}\text{Na}$ ,  $^{57}\text{Co}$ , and  $^{137}\text{Cs}$  and their characteristic energies of 122, 511, 662, and 1275 keV were used for calibration through experiments. Figure 7 shows the energy responses of a pixel in the corner, an edge pixel, and a center pixel to the  $^{22}\text{Na}$  source. The calibration result of the positive center pixel is also shown as a typical result. The energy resolution of each layer was evaluated using the total energy spectrum obtained from all pixels. The mean energy resolution of the scatterer was 20.63% at 122 keV, 7.64% at 511 keV, 6.34% at 662 keV, and 4.64% at 1275 keV, and the mean energy resolution of the absorber was 24.12% at 122 keV, 8.44% at 511 keV, 7.99% at 662 keV, and 5.97% at 1275 keV. The trend of the energy resolution was fitted by the following formula:

$$\delta_j = \frac{k_j}{\sqrt{E}} + l_j, \quad \#(19)$$

where  $j$  denotes the  $j^{\text{th}}$  layer. The results in Figure 8 indicate that  $k_j$  was 2.727 for the scatterer ( $j = 1$ ) and 3.020 for the absorber ( $j = 2$ ), and  $l_j$  was  $-0.0345$  for the scatterer ( $j = 1$ ) and  $-0.0359$  for absorber ( $j = 2$ ). For the characteristic energy of  $^{60}\text{Co}$  (1.33 MeV), the expected energy resolution was 4% and 5% for the scatterer and absorber, respectively. For a typical high energy of 4.44 MeV used in hadron therapy based on  $^{12}\text{C}$  de-excitation, the expected energy

resolution was approximately 1% for both layers.

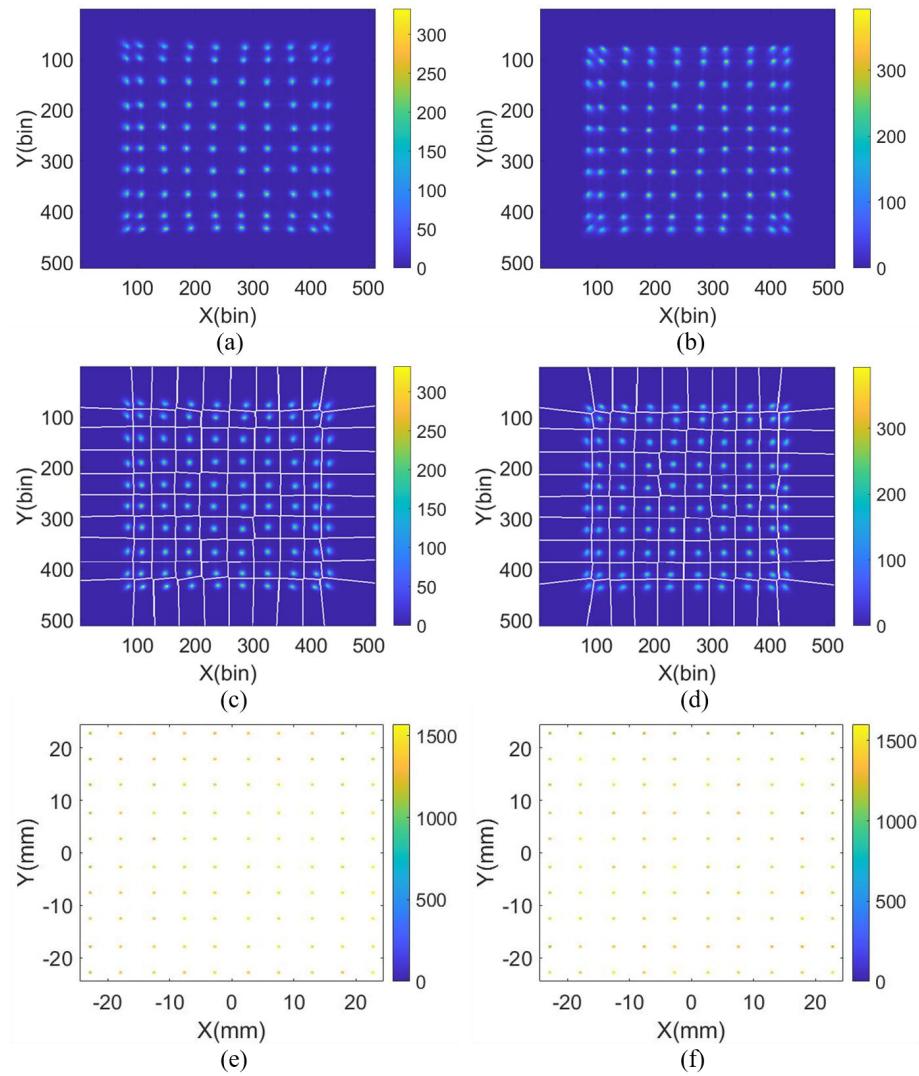


Figure 6. (a, b) Initial scatterplots of the scatterer and absorber from  $^{22}\text{Na}$  obtained using the decoding Equations (1)–(4). (c, d) Voronoi diagram of each layer. (e, f) Corresponding decoding interaction positions.

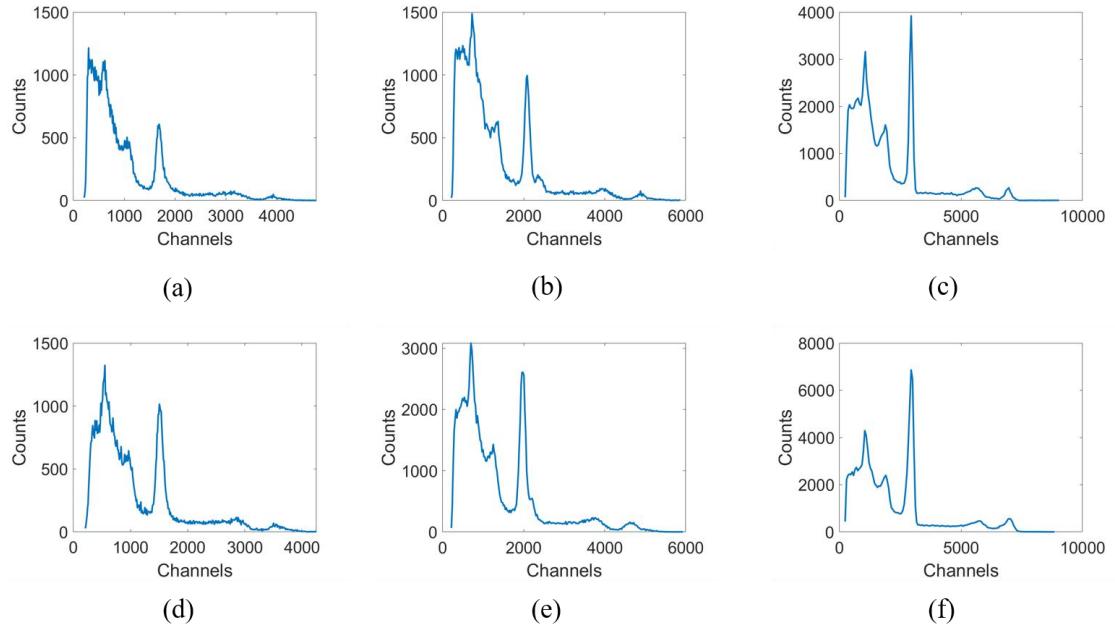


Figure 7. Partial results of the single-pixel energy spectra of  $^{22}\text{Na}$ : (a–c) corner, edge, and center pixels of the scatterer, respectively; (d–f) corner, edge, and center pixels of the absorber, respectively.

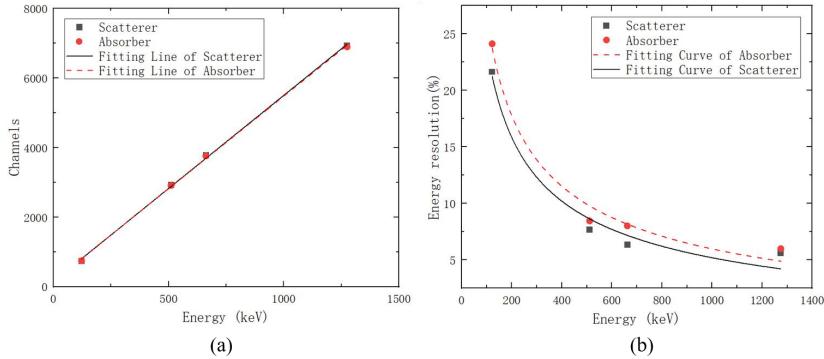


Figure 8. Spectral performance of the scatterer and absorber measured using the prototype at four energies (122, 511, 662, and 1275 keV) of  $^{22}\text{Na}$ ,  $^{137}\text{Cs}$ , and  $^{57}\text{Co}$ : (a) linear relationship between energies and channels; (b) measured energy resolutions and fitting curves.

### 3.2 Simulations

As shown in Figures 9 and 10, the CC distinguished and accurately reconstructed the spatial positions of the radioactive sources. The angular resolution of the CC was approximately  $5.5^\circ$  in the region close to the center of the FOV but was degraded to approximately  $8^\circ$  at the edge of the FOV. The proposed CC had good performance, i.e., a uniform and high angular resolution in the region of  $-50^\circ$  to  $50^\circ$ . Figure 11 shows the reconstruction results of the point-like source at three characteristic positions, which were compared with the results of the prototype experiments.

Table 1 presents the trend of the angular resolution with respect to the distance between the source and the scatterer. The FWHM decreased as the distance increases but of which the downward trend becomes stable. Tables 2 and 3 present the angular resolutions of circular plane

sources of different radii and the angular resolutions of point sources of different energies, respectively. As the radius of the source increased, the FWHM increased. Meanwhile, the FWHM decreased as the energy increased for both single-energy sources and multiple-energy sources.

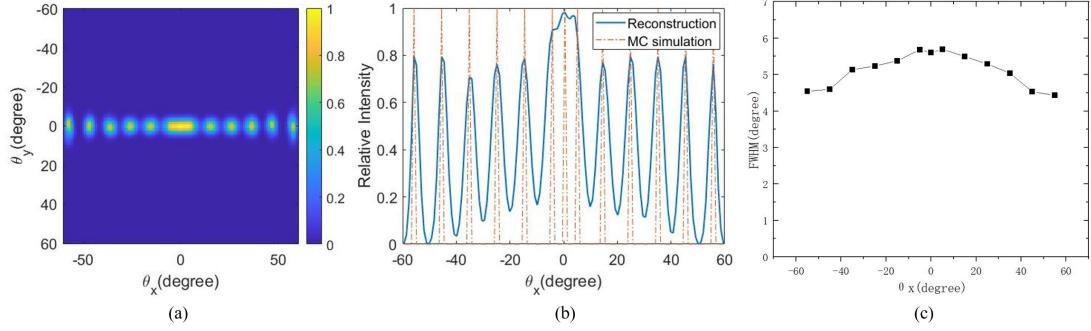


Figure 9. Reconstruction results obtained with the point-like source placed at different lateral positions in the simulations: (a) joint two-dimensional images; (b) profiles along the  $x$ -axis; (c) FWHMs of the corresponding positions.

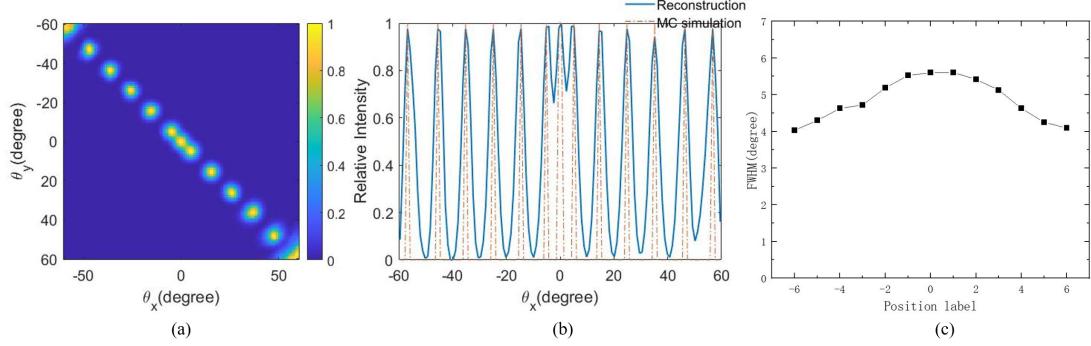


Figure 10. Reconstruction results obtained with the point-like source placed at different positions along the diagonal of the FOV in the simulations: (a) joint two-dimensional images; (b) profiles along the diagonal line; (c) FWHMs of the corresponding positions.

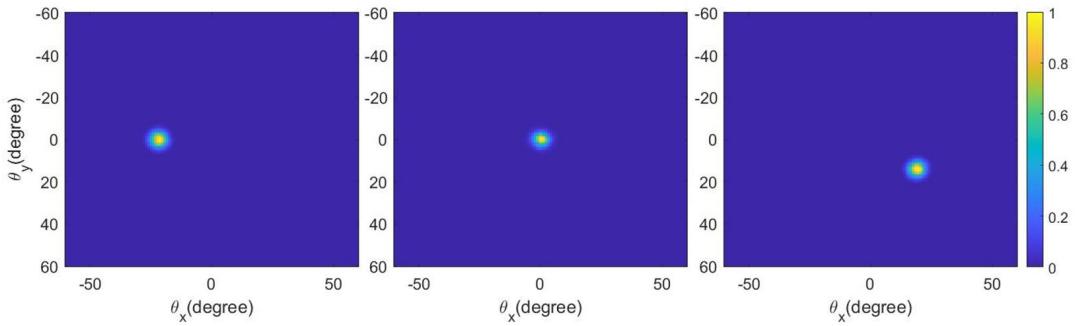


Figure 11. Reconstruction results for the point-like source at three positions in the simulations.

Table 1. FWHMs (degrees) for the reconstructed radioactive source ( $^{137}\text{Cs}$ ) at different distances (cm).

Distances	5	6	7	8	9	10	15	20	50	100
FWHM	5.60	5.48	5.21	5.46	5.40	5.10	4.93	4.75	4.63	4.45

Table 2. FWHMs (degrees) for reconstructed radioactive sources ( $^{137}\text{Cs}$ ) of different radii (cm).

Distances	0.5	1	1.5	2	3	4	5
FWHM	5.17	5.70	6.05	6.29	7.96	8.55	10.81

Table 3. FWHMs (degree) for reconstructed radioactive sources of different energies (keV) at 5 cm.

Energy	511	662	1275	50%511 50%662	50%662 50%1275	50%511 50%1275	64.3%511 35.7%1275
FWHM	6.35	5.60	5.23	5.65	5.389	6.053	6.25

### 3.3 Experiments

As shown in Figure 12, the reconstruction results obtained using the LaBr<sub>3</sub> CC were consistent with the simulation results. Table 4 indicates that the deviations between the reconstruction positions and exact values in the three experiments were  $<1.5^\circ$ . Additionally, as shown in Table 5, the FWHMs of the reconstructed radioactive source at three different positions of the  $^{137}\text{Cs}$  point-like source experiments agreed well with those of the corresponding simulations. The preliminary experimental results indicated that the angular resolution was approximately  $6^\circ$ . However, limited by the activity of the  $^{137}\text{Cs}$  source and the measurement time, the number of coincidence events obtained in our experiments was only several hundred. Thus, the reconstruction image would have relatively large amounts of noise and artifacts owing to the small amount of projection data [33]. As shown in the rightmost frame of Figure 12, which presents the source placed in  $P_d$ , because the sensitivity here was lower than that at the center of the FOV, the number of detected events was the smallest among the three positions. The deviation of the projection data, including the interaction positions and deposited energies, as well as the fewer statistics, led to reconstruction with more significant artifacts compared with the two other positions.

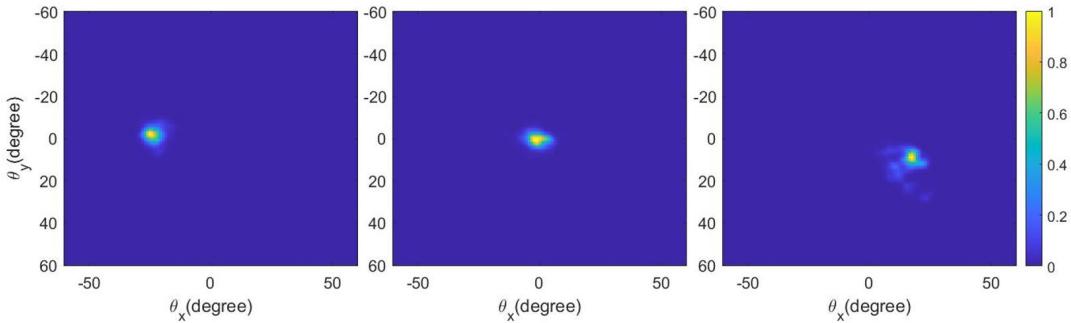
Figure 12. Reconstruction results for the  $^{137}\text{Cs}$  point-like source with the fabricated LaBr<sub>3</sub> CC prototype at three positions.

Table 4. Deviations (degree) between the reconstruction positions and exact values in the experiments.

Positions	$P_{l_2}$	$P_c$	$P_{d_2}$
Exact	(-25,0)	(0,0)	(15, -15)
Reconstruction	(-24.09, -1.42)	(-1.42, 0.47)	(15.59, 13.70)

Table 5. FWHMs (degree) of the reconstructed radioactive source at three different positions for the MC simulations and prototype experiments presented in Figures 11 and 12, respectively.

Positions	$P_{l_2}$	$P_c$	$P_{d_2}$
Simulations	5.28	5.60	5.74
Experiments	5.56	6.10	6.38

#### 4. Discussion

In this study, we designed and developed a two-layer LaBr<sub>3</sub>-based CC with a large pixel size and evaluated the performance of our prototype through MC simulations and experiments. We used an LUT to acquire list-mode data and the SD-OE-RR algorithm to reconstruct images for evaluating the feasibility of the CC prototype.

To spatially cluster the energy-depositing events in the crystal unit, the Voronoi diagrams and LUTs were created. For each layer, 4-channel voltage signals representing the number of scintillation photons were output in every time window, and the locating method used in Anger cameras was used to decode the 4-channel data. Finally, we created a scatterplot of energy-depositing events. The centroids of the crystal units were selected to be the interaction positions of events decoded in the corresponding area in the scatterplot for achieving the optimal estimation. The Voronoi diagrams and LUTs were created for clustering events. In the Voronoi diagrams, the distance from any point in each separated area to the seed point in this area was the shortest among the distances to all the seed points, which was the principle we used to cluster events. We selected the most representative points in the bright points by seeking peaks in the processed scatterplots and created the Voronoi diagrams for both the scatterer and absorber. Then, the LUTs were created accordingly. However, the whole complex process was based on nonstandard scatterplots owing to the hardware and structure. We used a light-absorbing material around the LaBr<sub>3</sub> crystal to differentiate the responses of the energy of edge pixels, resulting in a relatively low-voltage signal with high noise in the edge pixels (shown in Figure 7). The resistances in the encoding circuit had a deviation of approximately 1%, introducing a spatial error in the decoding process. Another defect was the incomplete correction for baseline drift of coding circuits, which caused an approximately 200-channel deviation in the voltage signals, affecting the decoding of both the position and energy.

The detection efficiency of the prototype for the <sup>137</sup>Cs point-like source used in our experiment was  $1.67 \times 10^{-3}$  at 662 keV. Compared with the LaBr<sub>3</sub>-based CC developed by the IRIS group of MACACO, the energy resolution of our prototype was slightly lower. This may

have been due to system defects of our CC. Because the  $\text{LaBr}_3$  crystal deliquesces easily, we used a 1-mm-thick glass plate and a 1.2-mm-thick Al shell for the vacuum packaging of each layer. The glass plate behind the crystal would absorb part of the scintillating photons, and the Al shell surrounding the crystal would cause Compton scattering of the gamma photons; both effects would lead to an incorrect value of the deposited energy and reduce the energy resolution. Additionally, the minor background radiation of  $^{138}\text{La}$  would influence the energy resolution [23, 34]. However, the natural abundance of  $^{138}\text{La}$  is approximately 0.09%, and it has a long half-life; thus, the influence of background radiation of  $^{138}\text{La}$  would be negligible. Furthermore, the overall energy resolution of our prototype was the average of the energy resolutions of all the pixels in the detectors. The energy response of the edge pixels would reduce the overall energy resolution owing to the structure of our prototype, as mentioned previously. As shown in Figure 13, the best energy resolution of the  $\text{LaBr}_3$  pixels in our CC was approximately 5% for 511-keV gamma rays, and the worst was approximately 15%. Thus, the overall energy resolution of the  $\text{LaBr}_3$  CC developed in this study is worse than that achieved in a previous experiment involving an  $\text{LaBr}_3$  scintillator detector (approximately 4%) [35] but comparable to the result of a simulation of a similar experimental situation [22]. Another example—the MACACO—is a similar  $\text{LaBr}_3$ -based CC to ours but employs a whole  $\text{LaBr}_3$  crystal and a 3-mm<sup>2</sup> SiPM array. Its angular resolution of approximately 5% was better than that of our CC owing to the advantages of its structure but was worse than that achieved in the previous experiment because the mutual decoding mode prevented it from achieving the ideal value. Although the energy resolution was affected by these system defects, our CC had a good energy resolution and is expected to achieve accurate nuclear material waste detection. In addition, if SiPMs larger than the scintillator array or one-to-one corresponding to the crystal array are used to reduce the loss of scintillation photons, the developed CC can achieve a better energy response of edge pixels.

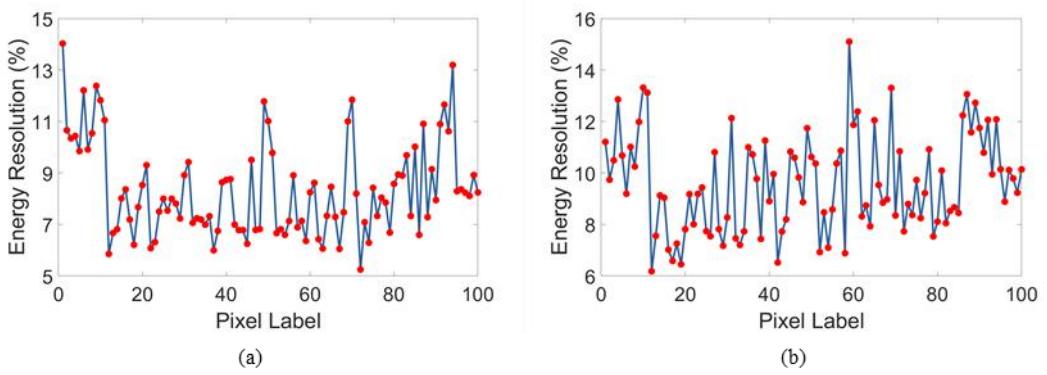


Figure 13. Energy resolutions of all the pixels in the developed  $\text{LaBr}_3$  CC prototype: (a) pixels in the scatterer; (b) pixels in the absorber.

The reconstruction simulation results indicated that the angular resolution of our CC improved when the sources were moved away from the center of the FOV, indicating that a larger scattering angle corresponded to a better resolution [36]. When the distances between the sources

and the scatterer increased, the angular resolution improved, which was consistent with the results of a previous study [32]. Two factors may have led to this phenomenon. First, the deviation of the scattering angle decreased as the distance increased, in accordance with Equation (13). Second, the system was more satisfied with far-field conditions, improving the resolution. Moreover, the angular resolutions of point sources improved slightly as the energy increased owing to the better energy resolution of higher energies. The imaging performance for sources of multiple energies exhibited a similar trend to that for single-energy sources, and the excellent simulation results for a real point-like  $^{22}\text{Na}$  (64.3% 511 keV and 35.7% 1275 keV) source indicated the applicability of the developed CC to nuclear decommissioning. The angular resolutions of circular plane sources worsened as the radii increased. For the point-like  $^{137}\text{Cs}$  source, the reconstruction results of our experiments agreed well with the simulation results, as shown in Table 2. The average FWHM of the reconstructed source was approximately  $6^\circ$  in the experiments and  $5.5^\circ$  in the simulation. Additionally, there was a small deviation in the reconstruction positions. The imaging results for the prototype indicated that in our experimental condition, a high energy resolution led to good imaging performance even though the spatial resolution was low owing to the large pixel size. Compared with a previously reported LYSO CC prototype using the same reconstruction algorithm, the performance of the  $\text{LaBr}_3$  CC was far better, even though the LYSO detectors had a small pixel size of 1 mm [17]. Similarly, in Dennis et al.'s study, the effects of the energy resolution on the performance were more pronounced than those of the spatial resolution in the case where the detected gamma energy was  $<2$  MeV [37]. The same trend was derived through a theoretical analysis using Equations (12) and (13). In our system, the radioactive source had a low energy of 662 keV—close to the static energy of the electron—which made the  $\Delta(c \cos \theta_i)_r$  part have a larger impact on the total deviation. Thus, when the CC is used for radioactive-material detection, improving the energy response may be more effective for enhancing the imaging performance than improving the geometric structure. In the case of a high energy resolution of the detector, a relatively loose restriction on the geometric structure to obtain a better sensitivity is allowed, as long as the CC system exhibited sufficient imaging performance for the expected applications. We investigated other CCs with large pixel sizes, such as a GAGG CC used in Fukushima to detect radioactive material [18, 19] and a CZT CC [38]. The GAGG CC has similar geometric parameters to ours, but its results were significantly worse than those achieved in our experiments, mainly owing to the poor energy resolution of the GAGG scintillator. In contrast, the MLEM reconstruction results of the CZT CC, whose pixel size was even larger than that of our CC, were comparable to the results of our experiments. This first-ever practical verification demonstrated that the two-layer  $\text{LaBr}_3$ -based CC with a large pixel size developed in the present study has a high angular resolution and good reconstruction performance, and it is expected to be used for radioactive source positioning in nuclear industry applications (e.g., nuclear decommissioning). Although its detection efficiency is

relatively low, our prototype indicates that a thicker crystal array can be used in future CCs, and the LaBr<sub>3</sub>-based CC is also expected to be used in nuclear medical imaging.

In future research, we will further evaluate the performance of our prototype in actual usage scenarios through more detailed experiments and simulations—with a focus on applications in nuclear decommissioning, natural radioactive background monitoring, and nuclear medical imaging. We will also optimize the structure of our CC, e.g., improving the packing mode and reducing the pixel size, to improve the performance of our prototype. A better technique for locating the position of interaction is also under consideration. A bilayer SiPM can be used in each layer to obtain not only the lateral position but also more accurate depth information of the events.

## 5. Conclusion

We developed a two-layer LaBr<sub>3</sub>-based CC prototype with a large pixel size, along with a highly efficient technique for determining interaction positions by decoding 4-channel voltage signals and performing clustering using Voronoi diagram-based LUTs. On the basis of the calibration of the energy response of each crystal pixel, we provided a framework for obtaining list-mode data of two-point events. The results of experiments and simulations indicated the developed CC prototype achieved an angular resolution of approximately 6° for a <sup>137</sup>Cs point-like source at 5 cm and a detection efficiency of  $1.67 \times 10^{-3}$ . The imaging performance of the developed prototype satisfies the requirements of radioactive source positioning in nuclear industry applications and the nuclear medical domain.

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## References

1. R. W. Todd, J. M. Nightingale, D. B. Everett, A Proposed  $\gamma$  Camera. *Nature* 251, 132–34 (1974).
2. Y. Kim, J. H. Kim, H. S. Lee et al., Development of Compton Imaging System for Nuclear Material Monitoring at Pyroprocessing Test-Bed Facility. *J. Nucl. Sci. Technol.* 53(12), 2040–48 (2016). doi:10.1080/00223131.2016.1199333.
3. Z. Yao, Y. Yuan, J. Wu et al., Rapid Compton Camera Imaging for Source Terms Investigation in the Nuclear Decommissioning with a Subset-Driven Origin Ensemble Algorithm. *Radiat. Phys. Chem.* 197, 110133 (2022). doi:10.1016/j.radphyschem.2022.110133.
4. J. Zhang, X. Liang, J. Cai et al., Prototype of an Array SiPM-Based Scintillator Compton Camera for Radioactive Materials Detection. *Radiat. Detect. Technol.* 3(3), 17 (2019). doi:10.1007/s41605-019-0095-1.
5. F. Tian, C. Geng, Z. Yao et al., Radiopharmaceutical Imaging Based on 3D-CZT Compton

Camera with 3D-Printed Mouse Phantom. *Phys. Medica.* 96, 140–48 (2022). doi:10.1016/j.ejmp.2022.03.005.

- 6. R. Wu, C. Geng, F. Tian et al., GPU-Accelerated Three-Dimensional Reconstruction Method of the Compton Camera and Its Application in Radionuclide Imaging. *Nucl. Sci. Tech.* 34(4), 52 (2023). doi:10.1007/s41365-023-01199-y.
- 7. Z. Yao, Y. Xiao, B. Wang et al., Study of 3D Fast Compton Camera Image Reconstruction Method by Algebraic Spatial Sampling. *Nucl. Instrum. Meth. A.* 954, 161345 (2018). doi:10.1016/j.nima.2018.10.023.
- 8. Z. Yao, C. Shi, F. Tian et al., Technical Note: Rapid and High-Resolution Deep Learning-Based Radiopharmaceutical Imaging with 3D-CZT Compton Camera and Sparse Projection Data. *Med. Phys.* 49(11), 7336–46 (2022). doi:10.1002/mp.15898.
- 9. M. Jan, I. Hsiao, H. Huang, Use of a LYSO-Based Compton Camera for Prompt Gamma Range Verification in Proton Therapy. *Med. Phys.* 44(12), 6261–69 (2017). doi:10.1002/mp.12626.
- 10. Z. Yao, Y. Xiao, Z. Chen et al., Compton-Based Prompt Gamma Imaging Using Ordered Origin Ensemble Algorithm with Resolution Recovery in Proton Therapy. *Sci. Rep.-uk.* 9(1), 1133 (2019). doi:10.1038/s41598-018-37623-2.
- 11. Z. Yao, Y. Xiao, J. Zhao, Dose Reconstruction with Compton Camera during Proton Therapy via Subset-Driven Origin Ensemble and Double Evolutionary Algorithm. *Nucl. Sci. Tech.* 34(4), 59 (2023). doi:10.1007/s41365-023-01207-1.
- 12. I. Kuvvetli, C. Budtz-Jørgensen, A. Zappettini et al., A 3D CZT high resolution detector for x- and gamma-ray astronomy. *Proc. SPIE.* 9154, 91540X (2014); doi:10.1117/12.2055119.
- 13. V.L. Ljubenov, P.M. Marinkovic. Applicability of Compton Imaging in Nuclear Decommissioning Activities. Paper presented at the International Yugoslav Nuclear Society Conference, Belgrade, Oct 2003.
- 14. T. Taya, J. Kataoka, A. Kishimoto et al., First Demonstration of Real-Time Gamma Imaging by Using a Handheld Compton Camera for Particle Therapy. *Nucl. Instr. Meth. A.* 831, 355-361 (2016). doi:10.1016/j.nima.2016.04.028.
- 15. E. Muñoz, J. Barrio, A. Etxeberria et al., Performance Evaluation of MACACO: A Multilayer Compton Camera. *Phys. Med. Biol.* 62(18), 7321 (2017). doi:10.1088/1361-6560/aa8070.
- 16. C.Z. Uche, W.H. Round, and M.J. Cree. Evaluation of Two Compton Camera Models for Scintimammography. *Nucl. Instrum. Meth. A.* 662(1), 55–60 (2012). doi:10.1016/j.nima.2011.09.058.
- 17. Z. Yao, Y. Xiao, M. Dong et al., Development of a Two-Layer Dense-Pixel LYSO Compton Camera Prototype for Prompt Gamma Imaging. *Phys. Med. Biol.* 68, 045008 (2023). doi:10.1088/1361-6560/acb4d8.
- 18. M. Uenomachi, Y. Mizumachi, Y. Yoshihara et al., Double Photon Emission Coincidence Imaging with GAGG-SiPM Compton Camera. *Nucl. Instrum. Meth. A.* 954, 161682 (2020). doi:10.1016/j.nima.2018.11.141.
- 19. Y. Shikaze, Y. Nishizawa, Y. Sanada et al., Field Test around Fukushima Daiichi Nuclear

Power Plant Site Using Improved Ce:Gd<sub>3</sub>(Al,Ga)5O<sub>12</sub> Scintillator Compton Camera Mounted on an Unmanned Helicopter. *J. Nucl. Sci. Technol.* 53(12), 1907–18 (2016). doi:10.1080/00223131.2016.1185980.

20. D. Y. Domínguez-Jiménez and H. Alva-Sánchez. Energy Spectra Due to the Intrinsic Radiation of LYSO/LSO Scintillators for a Wide Range of Crystal Sizes. *Med. Phys.* 48(1), 1596–1607 (2021). doi:10.1002/mp.14729.
21. S. Liprandi, M. Mayerhofer, S. Aldawood et al., Sub-3mm Spatial Resolution from a Large Monolithic LaBr<sub>3</sub> (Ce) Scintillator. *Curr. Dir. Biomed.* 3(2), 655–59 (2017). doi:10.1515/cdbme-2017-0138.
22. W. Lu, L. Wang, Y. Yuan et al., Monte Carlo Simulation for Performance Evaluation of Detector Model with a Monolithic LaBr<sub>3</sub>(Ce) Crystal and SiPM Array for  $\gamma$  Radiation Imaging. *Nucl. Sci. Tech.* 33(8), 107(2022). doi:10.1007/s41365-022-01081-3.
23. H. Cheng, B. Sun, L. Zhu et al., Intrinsic Background Radiation of LaBr<sub>3</sub>(Ce) Detector via Coincidence Measurements and Simulations. *Nucl. Sci. Tech.* 31(10), 99(2020). doi:10.1007/s41365-020-00812-8.
24. R. Shi, X. Tuo, H. Li et al., Unfolding Analysis of LaBr<sub>3</sub>:Ce Gamma Spectrum with a Detector Response Matrix Constructing Algorithm Based on Energy Resolution Calibration. *Nucl. Sci. Tech.* 29(1), 1(2017). doi:10.1007/s41365-017-0340-6.
25. Z. Yao, Z. Chen, S. He et al., Simulation Study of Interaction Position Correction for Compton Camera Based on Origin Ensembles with Subdivision Grid and Transmission Probability. Paper presented at the IEEE Nuclear Science Symposium and Medical Imaging Conference (NSS/MIC), Manchester, UK, 1–3 2019. doi:10.1109/NSS/MIC42101.2019.9059666.
26. A. Andreyev, A. Celler, I. Ozsahin et al., Resolution Recovery for Compton Camera Using Origin Ensemble Algorithm. *Med. Phys.* 43(8), 4866–76 (2016). doi:10.1118/1.4959551.
27. H. O. Anger, Scintillation Camera with Multichannel Collimators. *J. Nucl. Med.* 5, 515–31(1964).
28. P. J. Green, R. Sibson, Computing Dirichlet Tessellations in the Plane, *Comput. J.* 21(2), 168–173 (1978). doi:10.1093/comjnl/21.2.168.
29. A. Sitek. Reconstruction of Emission Tomography Data Using Origin Ensembles. *Ieee. T. Med. Imaging.* 30, 946–56 (2010). doi:10.1109/TMI.2010.2098036.
30. C.E. Ordonez, W. Chang, A. Bolozdynya. Angular Uncertainties Due to Geometry and Spatial Resolution in Compton Cameras. *Ieee. T. Nucl. Sci.* 46(4), 1142–47 (1999). doi:10.1109/23.790848.
31. A. Andreyev, A. Sitek, A. Celler. Fast Image Reconstruction for Compton Camera Using Stochastic Origin Ensemble Approach. *Med. Phys.* 38(1), 429–38 (2011). doi:10.1118/1.3528170.
32. M.A. Alnaaimi, Dissertation, University College London, 2011.
33. H. Rohling, M. Priegnitz, S Schoene et al. Requirements for a Compton camera for in vivo range verification of proton therapy. *Phys. Med. Biol.* 62(7), 2795(2017). doi:10.1088/1361-6560/aa6068

34. B.D. Milbrath, J. McIntyre, R. Runkle et al., Contamination in LaCl<sub>3</sub>:Ce Scintillators. United States. doi:10.2172/881704.

35. D.R. Schaart, S. Seifert, R. Vinke et al., LaBr<sub>3</sub>:Ce and SiPMs for Time-of-Flight PET: Achieving 100 Ps Coincidence Resolving Time. *Phys. Med. Biol.* 55(7), N179 (2010). doi:10.1088/0031-9155/55/7/N02.

36. C. Ordonez, W. Chang, A. Bolozdynya. Angular Uncertainties Due to Geometry and Spatial Resolution in Compton Cameras. *Ieee. T. Nucl. Sci.* 3, 1142–47(1999). doi:10.1109/23.790848.

37. D. Mackin, J. Polf, S. Peterson et al., The Effects of Doppler Broadening and Detector Resolution on the Performance of Three-Stage Compton Cameras. *Med. Phys.* 40(1), 012402 (2013). doi:10.1118/1.4767756.

38. Y. Liu, J. Fu, Y. Li et al., Preliminary Results of a Compton Camera Based on a Single 3D Position-Sensitive CZT Detector. *Nucl. Sci. Tech.* 29, 145 (2018). doi:10.1007/s41365-018-0483-0.